

# A Review: Formulation and Evaluation of Pharmaceutical Gel

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DOI: 10.47750/pnr.2022.13.S01.160

## Abstract

The review's goal is to make and survey a drug gel made of both normal and counterfeit polymers. Gel measurements structures function admirably as medication conveyance techniques since they accommodate exact medication discharge control and natural security for the drugs. Various physicochemical parts of the gel that influence its attributes are likewise explored. We have accumulated sources from recently distributed examination and survey articles. We gathered data from 20-25 papers. Drug gel is surveyed for its capacity to gel, for its solidarity, for its bioadhesion, for its spreadability, for microbiological research, and for in vitro discharge. Because of our exploration, we have arrived at the resolution that skin medicine conveyance is an engaging procedure for both nearby and foundational medicines and is regularly utilized in the administration of provocative ailments such dermatological illnesses and outer muscle wounds. The perils associated with the different conditions of retention, for example, pH changes, the presence of proteins, and gastric exhausting time, are kept away from by effective arrangement, alongside the dangers and burdens of intravenous treatment and gastrointestinal infections. Furthermore, the medication has a higher bioavailability and acts at the activity site right away. The gel not entirely settled to be an extremely encouraging option for skin or transdermal treatment. To completely grasp the course of drug gel-incited wound recuperating, more examination should be finished.

**Keywords-** Topical formulation, Pharmaceutical gel, transdermal drug delivery, targeted therapy

## INTRODUCTION

The administration of drugs to the human body by many routes, including oral, sublingual, rectal, parental, cutaneous, inward breath, and so on, has proved successful in treating illness. Skin conveyance can be defined as the application of a medication containing specific details to the skin in order to directly treat cutaneous issues like skin breakouts or the cutaneous symptoms of an underlying illness like psoriasis with the goal of limiting the medication's pharmacological or other effects to the skin's outer layer or inside the skin. Although froths, splash, drugged powders, arrangements, and, unexpectedly, cured glue frameworks are being utilised, semi-strong plans in all of their varieties overwhelm the framework for efficient conveyance. Skin definitions are probably among the most difficult elements to design since they describe how a drug is delivered to a specific location. In order to accommodate varied combinations that may have different, if not opposing, physicochemical properties, a practical effective detailed must provide a stable synthetic environment in a reasonable distribution holder. An efficient definition should interact with the skin climate when applied because this may affect how quickly the structures arrive to achieve adequate skin absorption.<sup>1</sup>

Delivery of medication to the skin provides a potent and targeted therapy for adjacent dermatological issues. This method of drug delivery has gained popularity since it avoids the first-pass effects, gastrointestinal discomfort, and metabolic degeneration caused by oral organisation. Due to the main prior effect, only 25–45% of the orally administered fraction reaches the blood stream. These unfavourable viewpoints may be avoided by using the gel definitions, which had been recommended as an application. Because they are less greasy and can be easily removed from the skin, effective gel formulations provide suitable delivery equipment for tablets. All things considered, Gels envelop stage device wherein inorganic waste are not disintegrated anyway essentially scattered all throughout the constant segment and large natural flotsam and jetsam are broken down in the persistent stage, haphazardly curled in

the adaptable chains. They are intended to be done to the skin or certain mucous films for protective, prophylactic or helpful capabilities.

### **1.1 Pharmaceutical Gel**

Typically, gels are constructed from a fluid stage that has been thickened with various components. They are frequently prepared under the direction of qualified gelling experts like HPMC, Carbopol, Sodium CMC, and others. In the detailing of gels, extra ingredients including stabilisers, antibacterial additives, and cancer-prevention compounds are used.<sup>2</sup>

The term "gel" comes from "gelatin," and both "gel" and "jam" may be traced back to the Latin words "gelu" for "ice" and "gel" for "freeze" or "harden." This introduction demonstrates the basic concept of a fluid setup to key regions of strength for a texture that doesn't drift but is adaptable and retains certain fluid aspects.

Gels are described as semi-unbending structures in which the growth of the scattering medium is restrained by a three-layered arrangement of intertwined waste products or solvated dispersed section macromolecules.

Gels are frequently viewed of as being more rigid than jams because they have more covalent crosslinks, thicker real bonds, or just less fluidity. Gel-shaping polymers provide materials with a variety of rigidities, ranging from a sol to an adhesive, jam, gel, and hydrogel as the rigidity increases. 5,6 Due to the fact that the compounds in some gel structures are either soluble or insoluble, or because they may form totals that scatter light, some gel structures are nearly as transparent as water while others are turbid. For certain exceptions, the attention paid to the gelling specialists is frequently much less than 10%, typically ranging from 0.5 to 2.5 percent.<sup>7,8</sup>

### **1.2. Route of penetration:**

Drug molecules come into touch with cellular waste, bacteria, and other substances on the skin's surface, which has an impact on penetration.

Three routes connect the administered medication to the living tissue:

1. Through the hair follicles
2. sweat ducts,
3. Continuous stratum corneum between the appendages, in that order (hair follicles, sebaceous glands, eccrine, apocrine glands and nails).

Only around 0.1 percent of the fragmentary limb area is available for transport yet it is essential for particles and large polar atoms. The essential border is the perfect layer corneum, and several upgrade techniques aim to disrupt or avoid this layer. Possible layers may start a prodrug or take a medicine. In general, deeper dermal regions seldom impact retention in a substantial way again. This method of medicine delivery has gained popularity since it prevents oral organization-related metabolic degeneration, gastrointestinal distress, and first-pass impact. The skin course of organisation has been employed to provide fundamental pharmacological outcomes or to give local results for treating skin problems.<sup>9, 10</sup>

The primary purpose of putting medicine to the skin to treat skin conditions is to cause a local reaction where it is applied. Most of the time, only a small percentage of the total quantity really makes it to the activity site, which results in constrained neighbourhood mobility. The very intriguing boundary qualities of the skin have made this a challenging effort.<sup>11</sup>

### **1.3. Structure of gels:**

The unbending property of gel is caused by the gelling expert who builds networks by connecting particles. 12, 13. Power type that controls the structure of the framework and the characteristics of the gel and is responsible for the connection of particles 3, 14. The single particles display spherical groups of moment atoms, isometric totals, or single macromolecules. GEL displays the gel networks' game strategy.

### **1.4. Advantages of gel formulations:**

The gel formulation has several key benefits over conventional semisolid dose formulations.<sup>15, 12</sup>

1. Compared to other formulations, gels are simple to manufacture.
2. Gel is a sophisticated, non-greasy composition.
3. Gels offer fantastic adhesion to the application region.
4. Gels are eco-friendly and biocompatible.
5. Be incredibly resilient to stressful situations.

### **1.5. Disadvantages of gel formulation:**

Despite having a number of benefits. Gel formulations can come with certain drawbacks..<sup>16, 17</sup>

1. Gels have a more gradual and persistent effect.
2. The additives or gelators could irritate people.
3. The risk of microbial or fungal assault on gel is increased by the presence of water.
4. The formulation's solvent loss dries to gel.
5. In some gels, flocculation results in an unstable gel.

### 1.6. Ideal properties of topical gel:

1. The gel ought to be uniform and transparent.
2. When shear or force is applied during the container's shaking, the gel should break easily.
3. The gel should have an inert composition.
4. The gel must not be sticky.
5. The gel shouldn't ever contact with another component in the formulation.
6. The gel must be reliable.
7. The skin or any area where the gel is placed shouldn't be irritated..<sup>18</sup>

### 1.7. Gel forming substances:

When fragmented in a fluid state as a colloidal mixture, gel-shaping professionals create a pitifully robust internal structure. They are hydrophilic inorganic compounds or natural hydrocolloids. As stabilisers and thickeners, gelling agents can also provide thickening without stiffness. Recently, polymers have been widely used as gelling experts in semisolid measuring structures. Among them, carbomers, which are designed macromolecular polymers of caustic acrylic, are frequently used because they exhibit excellent thickening ability across a wide pH range. The gel-shaping expert, who is often a polymer in small concentrations, produces a semisolid consistency in the definition that slows down the rate of seepage of the detailing and extends the amount of time spent at the organisation site.<sup>19</sup>

#### 1.7.1. Natural polymer:

Corrective applications have often used regular polymers. They have several purposes, including cosmetics, skin and hair care, as well as modifiers and stabilisers, and are biocompatible, safe, eco-friendly, and incredibly alluring to consumers. Polysaccharides, starch, thickener, guar gum, carrageenan, alginate, gelatin, gelatine, agar, collagen, and hyaluronic acid are among the most often used natural polymers and are of exceptional importance. Starches are naturally occurring polysaccharides that may be used in a variety of forms, particularly as granule and solvent starches.<sup>22</sup>

**Table 1: Natural Gelling Agent Polymer For Pharmaceutical Preparation**

Polymer Name	Chemical Nature	Pharmaceutical Application	References
Agar	Agarobiose (D-galactose/Agaropectin) is also known as agarose and agaropectin.	Gelling suppositories, suspending agents, emulsifying agents, laxatives, bacterial cultures, and surgical lubricants are some examples of tablet disintegrants.	Kulkarni et al.,(2012) [23]
Aloe Gel	Gelling suppositories, suspending agents, emulsifying agents, laxatives, bacterial cultures, and surgical lubricants are some examples of tablet disintegrants.	Sustained Release Direct Compressible Matrix Tablets.	Alonso et al.,(2009) Hamman et al.,(2008), Ahad et al.,(2010) [24,25,26]
Albumin	Plasma protein is made up of three homologous domains and has 585 amino acids in human serum albumin (I,II,III)	Gene delivery, injection, creation of nanoparticles, and medication administration (based on peptide or protein).	Langer et al.,(2003)[27]
Alginate acid	A naturally occurring, edible polysaccharide found in brown algae is alginate acid, often known as algin.	Alginate acid is frequently used to stabilise oil-in-water emulsions as well as thicken and suspend a variety of pastes, creams, and gels.	Suhail et al.,(2021)[28]
Arginine	an amino acid that aids in the body's protein synthesis.	Arginine is essential for immune system	IUPAC-IUB Joint Commission on

		function, hormone production, wound healing, ammonia removal from the body, and cell division.	Biochemical Nomenclature [29]
Chitosan	One of the most prevalent natural polysaccharides is chitin.	Due to its useful qualities, including its antibacterial activity, non-toxicity, simplicity of modification, and biodegradability, chitosan is a bioactive polymer with a wide range of uses.	Demchenko et al.,(2022)[30]
Carrageenans	Repeating galactose units, 3,6-anhydrogalactose (3,6-AG), and alternating (1-) and (1-4) glycosidic linkages joined by sulfated and non-sulfated sugars	Soft and Hard Gel Hand lotions, shampoos, emulsions, dressings, antacid gels, topical bases, suppository bases, contraceptive gels, and controlled-release tablets	Lev et al.,(1997), Kadajji et al.,(1972) Khalil et al.,(2017) [31,32,33]
Dextran	$\alpha$ -D-1,6-glucose-linked Glucan	spheres or implants made of hydrogel	Wolthuis et al.,(1997), Jong et al.,(2001) [34,35]
Guar gum	Guar gum can be a cost-effective alternative because of its good viscosity and spreadability.	Guar gum is frequently used in the food industry as a gelling and emulsifying agent since it produces a nice gel at low concentrations (between 0.5 and 1 percent) and achieves its greatest viscosity at low temperatures.	Jantrawut et al.,(2014)[36]
Gelatin	Combination of Polypeptide Chains of Glycine, Proline, and Hydroxyproline from Purified Protein Fractions	One of the most used gelling agents is gelatin. Film Formation/Rapid Dissolution	Hathout et al.,(2019)[37]
Hemicellulose	(Mannans/Xyloglucans/Xylans)/-1,4-Linked Dglycans/Xyloglucans	Agent for Forming Film	Cosgrove et al.,(2005) [38]
Hyaluronic acid	N-Acetyl glucosamine, Glucuronic Acid, and Polyanionic Polysaccharide	Eye gel, prolonged drug release, intra-articular injections, and artificial insemination	Ying et al.,(2019), Kwon et al.,(2019)[39,40]
Hydroxyethyl Cellulose	Closure Ethers	Tablet Film Forming, Binders, Coating Agents, Emulsifying	Lin et al.,(2020), Demina et al.,(2020)[41,42]

		Agents, and Stabilizing Agents	
Inulin	Glucofructan oligomer mixture, polysaccharide, and polymers that have been derivatized using succinic and methacrylic anhydrides	Methylated inulin hydrogels and film formers	Wan et al.,(2020) [43]
Pectin	Anionic Polysaccharide -1, 4-Linked D-galacturonic Acid	Tablets (Directly Compressed, Sustained-Release, Gel Bead, Injection, Oral Film, Colon-Drug Delivery System, Transdermal Patch)	Reddy et al.,(2020), Zhang et al.,(2019), Ogunsona et al.,(2018) [44,45,46]
Sodium Alginate	D-Mannuronic acid and L-guluronic acid in homopolymers, as well as D-Mannuronic acid and L-guluronic acid connected by - or -1,4 glycosidic linkages and sodium salts of these compounds	Tablet binders, Tablet Disintegrants, Colloidal Preparation, Thickening, Stabilizing, Suspending, Gel Producing, Emulsion Stabilizing, and Biopolymer Film	Afshar et al.,(2020), Hasnain et al.,(2020)[47,48]

### 1.7.2. Semi-synthetic polymers

Two major groups of cellulose derivatives with different physicochemical and mechanical characteristics are cellulose ethers and cellulose esters. Cellulose derivatives possess qualities including uniformity in arrangement, surface action, thermoplastic film characteristics, and resistance to oxidation, biodegradation, and intense hydrolysis. The cellulose ethers (such as methylcellulose, ethyl cellulose, hydroxyethyl cellulose, hydroxypropyl methylcellulose, carboxymethyl cellulose, and sodium carboxymethyl cellulose) can be dissolved in water, in contrast to the cellulose esters (such as cellulose acetic acid derivation, cellulose acetic acid derivation phthalate, cellulose acetic acid derivation butyrate, cellulose acetic acid.<sup>49</sup> These polymers are mostly used in cosmetic items including creams, shampoos, salves, and gels as gelling, bioadhesive, thickening, and balancing out agents. Compared to common gelling specialists such starches, acacia, sodium alginate, agar, gelatin, and gelatin, they are less susceptible to microbial contamination.<sup>50</sup>

**Table semi-synthetic polymers**

Polymer	Properties	reference
Nitrocellulose	Film development and prolonged product wear	Tafuro et al.,(2019)[51]
Acrylate-copolymers	upgraded product design	Penzel et al.,(2000)[52]
Hydroxypropyl methylcellulose	Film development and prolonged product wear	Silva et al.,(2005)[53]
Hydroxyethyl cellulose	Rheological control and simplicity of use	National Center for Biotechnology Information [54]
Polyacrylic-acid	prolonged shelf life of the product	Ohara et al.,(2021)[55]
Polyamides	extended product wear, improved product shelf life, rheological control, and simplicity of application	Patil et al.,(2013)[56]
Cellulose – Derivatives	Solution viscosity and surface performance	Iunchedii et al.,(2002) [57]
Cellulose acetates	Topologies of thermoplastic films and heat resistance	Mohite et al.,(2014) [58]
Cellulose nitrates	Biodegradation, hydrolysis, and oxidation	Costa et al.,(2019) [59]

Chitosan	Anti-inflammatory antioxidant, antifungal, and antimicrobial	Iijima et al.,(2014) [60]
Collagen	serve as a fibroblast's compass.	Goddard et al.,(1999) [61]
Gelatin	uses water to create thermally reversible gels	Sarangi et al.,(2018) [62]
Pectin	Commercially produced as a white to light brown powder, mostly derived from citrus fruits, and used as a gelling ingredient in food, especially in jams and jellies.	Muruges et al.,(2013)70 [63]
Liven	animal-free components for proteins	Halasa et al.,(1981)[64]
Silk	wholesome protein fibre	Zheng et al.,(2021)[65]

**1.7.3. Synthetic polymers:** Carbomer is a synthetic polymer from the Carbopol family. It is the polymer that is used the most frequently in gel arrangement. In the 1950s, carbopols were initially introduced and used for gels. They are used to create an acidic pH 3 arrangement in water and have a powdered structure with high bulk densities. With a higher pH, they thicken (5-6). Within the sight of a flowing arrangement, they can blow up to many times in volume. The thickness of carbopol arrangements ranges from 0 to 80,000 centipoise. Carbomer, poloxamer/surfactants, and polyacrylamide are a few examples of designed gel-framing polymers.

#### Synthetic polymers and their biomedical applications

Synthetic polymer	Biomedical application	Commercial product and company name	References
Poly (vinyl)alcohol (PVA)	suitable for vascular cell culture, tissue mimicry, and vascular implanting	appropriate for tissue mimicry, vascular cell culture, and vascular implant	Jiang et al.,(2011) [66]
Carbomer	used to increase the biological availability of medicines and regulate their release.	In various applications, carbomers are frequently used as a bioadhesive.	Hosmani et al.,(2006)[67]
Poly(ether urethanes)	Heart valves, blood-contacting equipment, coatings, and vascular grafts.	Precision Spectra, an implantable neurostimulator, is used for (Boston Scientific)	Shastri et al.,(2003) [68]
Carbopol 934	suitable for usage in lotions and creams as a rheology modifier	Cross-linked polyacrylic acid polymer, carbopol 934, is a white powder. It has a creamy taste profile and short flow characteristics.	Ubaid et al.,(2016)[69]
Polyphosphazenes	Controlled medication distribution through implants and in tumor-bearing animals	Cardioverter defibrillator implantable ENERGEN (Boston Scientific)	Schacht et al.,(1996) [70]
Carbopol 940	In gel preparations, carbopol 940 is frequently employed as a gelling agent.	To create a high-quality gel preparation, carbopol 940 concentration needs to be taken into consideration.	Safitri et al.,(2021)[71]
Carbopol 941	It is possible to create low-viscosity	Crosslinked polyacrylic acid polymer is a white	Muramatsu et al.,(1996)[72]

	lotions and gels with high clarity using the carbopol 941 NF polymer.	powder. It is intended to suspend, maintain, and improve the visual appeal of low viscosity materials.	
Poly(ethylene glycol) (PEG)	Hydrophilic linear polymer utilised as pore forming in dialysis membranes, hydrogel, or as an antifouling coating on catheters	PEGDM 1.0 (Polysciences, Inc.)	Woerly et al.,( 1998) [73]
Polyurethane	materials that are frequently utilised to make blood-contacting devices like heart valves or synthetic veins and arteries	PCU Bionate (long-term use in the body and has been used in chronic implants) SPU Biospan TSPCU CarboSil (exceptional toughness and biocompatibility) ethylene TPU (long-term implantation)	Burke et al.,(2004) [74]
Poloxamers	Due to their commercial availability, wide variety of molecular weights, unusual behaviour, and flexibility, poloxamers are an advantageous option in pharmaceutical technology and the biomedical field.	A group of non-ionic, water-soluble triblock copolymers called poloxamers are made of polar (poly ethylene oxide) and non-polar (poly propylene oxide) building blocks.	Aguilar et al.,( 2007)[75]
Polyimides	Neuroprosthetics using Implantable Pulse Generators for Deep Brain Stimulation	Surgical Implantable Neurostimulator (Boston Scientific)	Teo et al.,(2016)[76]
Poly(caprolactone diol) (PCL)	Diol for making polyurethane	13 PURASORB PC (Corbion)	Ferreira et al.,(2008)[77]
Polyvinylchloride (PVC)	Blood bags and blood tubes	Blood tubing set NiproSet (NIPRO)	Maitz et al.,(2015)[78]
Poly(carbonate) (PC)	Biodegradable polyester for containers and dialysis membranes	Makrolon (Covestro)	Newehy et al.,(2011)[79]

**1.7.4. Miscellaneous gel-forming polymers:** Clays, beeswax, microcrystalline silica, cetyl ester wax, aluminium stearate, and beeswax are a few examples of different polymers that produce gels.<sup>80</sup>

### 1.8. Method for preparation of gel:

There are three techniques for making gels.

- 1. Fusion technique:** This method involves blending the drugs, components, gelling stores, and vehicles at a high temperature till a semi-firm texture is achieved.
- 2. Cold method:** In this method, all of the ingredients, excluding the medication or active pharmaceutical component, are heated and mixed simultaneously. The temperature of the mixture is then lowered, the drug is added, and the blending process is repeated until the gel has not formed.
- 3. Dispersion approach:** This procedure involves mixing the gelling agent with water until it begins to swell, at which point the medicine is dissolved in the medium and added to it. If necessary, add buffer solution to the gel

to change the pH.<sup>81</sup>

### 1.9. Mechanism of gel formation:

Three different forms of cross-linking create gels.<sup>82,83</sup>

- a) Chemical cross-linking
- b) Physical cross-linking
- c) Ionic cross-linking

#### a) Chemical cross-linking:

Similar synthetic cross-connecting is observed in polymers that have unprotected bunches in their structure. When a cross-connecting component is used in such polymers, the free gathering and the added portion experience an irreversible substance reaction. This irreversible reaction results in an increase in consistency, and after reaching a certain point, a gel is formed, such as complex cross-connecting gels made of polyacrylic acid (with several carboxylic acids) and glycols (containing hydroxyl groups).<sup>84</sup> Fig. 4 depicts the chemical cross-linking process.

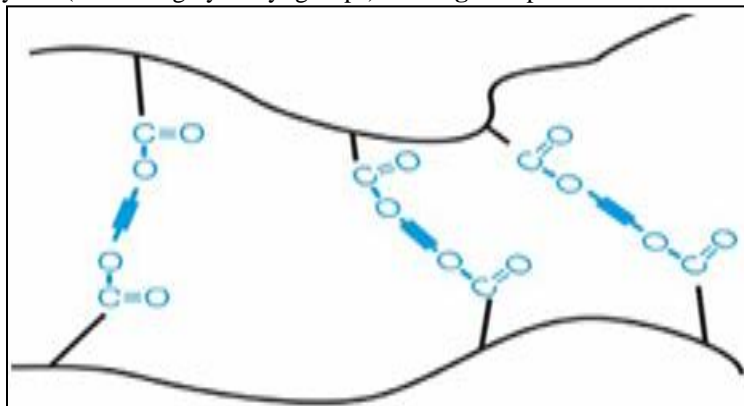


FIG. 4: CHEMICALLY CROSS-LINKED GEL

#### b) Physical cross-linking:

In some circumstances, the transition from a solution to a gel can happen due to the creation of hydrogen bonds, the solubilization of crystalline components, concentration changes, temperature changes, or hydrophobic interactions. Dextran gels, poly (N-isopropyla crylamide) gels, cellulose gels, and others are examples of these gels.<sup>85</sup> Physical cross-linking is shown in Fig. 5.

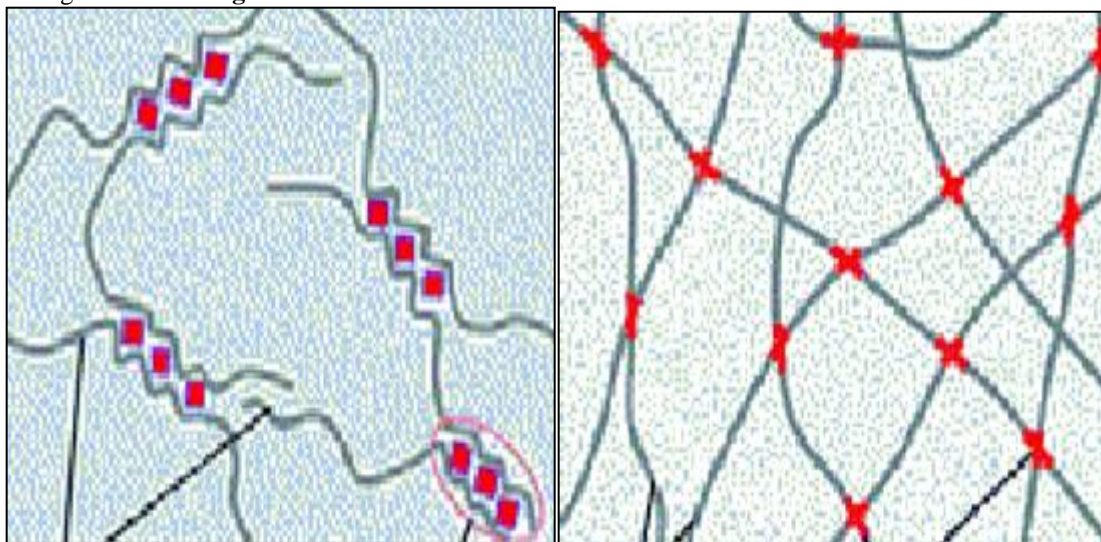


FIG. 5: PHYSICALLY CROSS-LINKED GEL

c) **Ionic cross-linking:** In order to create a gel, charges can be formed on polymers or other molecules (solvents) to promote cross-linking (Fig. 6). The charges on such molecules cause them to form ionic connections. In the presence of calcium ions, polysaccharide alginate, for instance, creates a gel matrix that may enclose certain components (enzymes, etc.). You may also achieve ionic gelation by changing the medium's pH. (solvent). Such mixes gel when the pH is changed; for instance, pectin gels when exposed to an acidic pH in a suitable medium.<sup>86</sup>

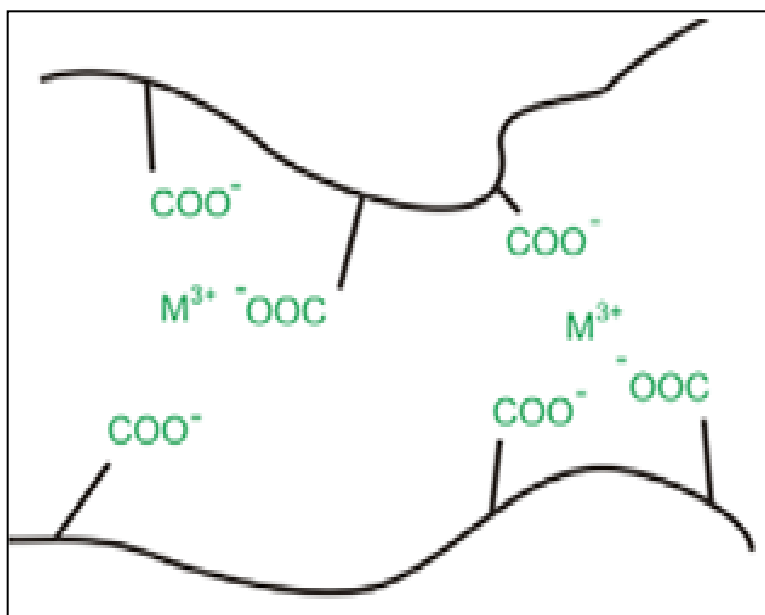


FIG. 6: IONIC CROSS-LINKING IN GEL

## 2.0. Classification of gel:

Pharmaceutical polymer gels are divided into groups according to their colloidal phase, solvent type, rheology, physical makeup, and method of drug administration.

### 2.1. On the basis of colloidal phase:

Inorganic two-stage framework (also known as polymer gels) and single-stage framework (natural gels). When particles form three-layered structures across the gel in the two-stage framework due of their relatively large molecule sizes in the dispersed stage, the gel mass is referred to as magma (e.g., bentonite magma). Two-stage frameworks typically contain floccules of tiny particles, which results in an unstable gel structure. Both magma and gel may have thixotropic framing semisolid properties while stationary, but when agitated, they transform into fluids in a single-stage framework, where large natural particles dissolve. These polymer gels might be made of natural gums, artificial polymers (like carbomer), semi-synthetic polymers (like cellulose subordinates), or both (e.g., tragacanth).<sup>80</sup>

### 2.2. On the basis of solvent:

Depending on the kind of solvent employed as the non-stop phase throughout the procedure, gels may be classified as hydrogels (water-based), organogels (non-aqueous solvent), oraerogels/xerogels.

**2.2.1. Hydrogel:** Hydro-gels are polymeric structures that absorb extreme water properties while remaining insoluble in fluid mixtures due to the substance or actual cross-linking of polar or nonpolar polymer chains. Hydrophilic hydro-gels exhibit a number of remarkable physicochemical properties that make them ideal for biomedical application as well as drug delivery, in contrast to hydrophobic polymeric organisations, such as poly (lactic acid (PLA) or poly (lactide-co-glycolide) (PLGA), that have limited water-ingestion capacities. Gels arrangement typically returns at room temperature, and natural solvents are hardly ever used. Hydro-gels will eventually be distinguished from the other hydrophobic polymers by in-situ gelation with cell and medicine exemplification capacities. The polymers used to make hydro-gels might be natural or synthetic. 88 Hydro-gels are three-layered frameworks that have been water-enhanced and are typically constructed of hydrophilic polymers. These are full-scale, pass-connected atomic structures that are insoluble but may expand swiftly in natural liquids.<sup>89</sup>

**2.2.2. Organogels:** A nonaqueous dissolvable serves as the persistent stage in organogels. Plastibase (low sub-atomic weight polyethylene broken down in mineral oil and stock cooled) and metallic stearate scatterings in oils are examples of organogel. An organogel is a thermoplastic (thermoreversible), non-translucent substance that is created from a fluid natural stage that is interconnected in three different ways. For instance, the fluid might be a naturally soluble substance, mineral oil, or vegetable oil. The flexible qualities and solidity of the organogel are significantly influenced by the solvency and molecular features of the organising. These frameworks frequently rely on the organising particles coming together on their own. Organogels have the potential to be used in a variety of goods, including food, cosmetics, medicines, and protection for the workplace. Wax crystallisation in unprocessed petroleum is one example of how an undesirable thermo reversible structure might arise.<sup>90</sup>

### 2.2.3. Xerogels and Aerogels:

Strong gels with a low dissolvable fixation, xerogels are frequently moulded by the disappearance of the gel's dissolvable components. They might be put back into gel form by adding a specialist who first absorbs the gel network before expanding it. Acacia tears, dry gelatin, dry cellulose tragacanth strips, and polystyrene are all examples of xerogels.

A xerogel is a robust form of gel that has a low pore size (150-900 m<sup>2</sup>/g), high floor place (25 percent), and inappropriate porosity (25 percent) (1-10 nm).

The xerogels can maintain their distinctive shape, but they frequently shatter as a result of the shocking shrinking that occurs while they are being dried. By using a higher temperature during the heating process, xerogel shrinks owing to a small quantity of thick float, which effectively transforms the permeable gel local region into a thick glass.

While maintaining the strong local area and changing the gel's fluid phase with fuel, an aerogel is produced with little to no gel shrinkage. It was initially seen in extremely critical conditions, but it is currently probable in broadly drying conditions as well. When the gel's dissolvable end occurs under extremely stressful conditions, the pass-connecting region doesn't shrink, and a highly permeable, thin aerogel is created as a result. In this way, the drying method will determine whether an aerogel or xerogel may be formed.<sup>80</sup>

### 2.3. Based on rheological properties:<sup>91</sup>

Gels typically have non-Newtonian flow characteristics. They are categorised as, Plastic gels

- a. Pseudo plastic gels
- b. Thixotropic gel

#### (a) Plastic gels:

**E.g.:** The yield value of the gels, which is at which the elastic gel bends and starts to flow, is shown on the rheogram plot for Bingham bodies, flocculated suspensions of aluminium hydroxide, which display plastic flow.

#### (b) Pseudo-plastic gels:

**E.g.:** Fluid scattering from substances like sodium alginate, tragacanth, Na CMC, and others reveals a pseudo-plastic stream. Without regard to yield value, the consistency of these gels decreases as the cost of shearing increases. The long chain particles of the straight polymers undergo a shearing motion, which produces the rheogram. The damaged atoms start to shift their extended hub toward skim with the release of dissolvable from the gel network as the shearing force is repeated.

#### (c) Thixotropic gels:

The incredibly weak bonds that hold gel particles together can be broken apart by shaking. Due to the particles colliding and re-connecting, the resulting arrangement will once again gel. (The isothermal gel-sol-gel transition that is reversible.) This takes place in a colloidal framework with non-round particles to create a design that resembles a platform.

**E.g.:** Agar, bentonite, and kaolin<sup>92</sup>

### 2. 4. Based on physical nature:

**(a) Elastic gels:** Agar, pectin, guar gum, and alginates gels all behave elastically. At the site of connection, the fibrous molecules are connected by relatively weak interactions, such as hydrogen bonds and dipole attraction. Additional bonding occurs through a salt bridge of type -COO-X-COO between two neighbouring strand networks if the molecule has a free -COOH group.

**E.g.:** Carbenate with Alginate

**(b) Rigid gels:** This can be created from macromolecules with a main valence bond connecting the framework. As an illustration, the Si-O-Si-O link holds the silica molecules in silica gel, creating a polymer structure with a network of pores.<sup>80</sup>

### 2.5. On the Basis of Drug Delivery:

Pharmaceutical gels are frequently employed in drug delivery systems as carriers. These gels might be categorised as:

#### 2.5.1. Sustained/controlled release gels:

Controlled medication delivery systems provide several advantages, including reduced dose recurrence, which improves patient compliance, maintenance of blood levels within a desirable range by limiting fixation fluctuation, restricted/designated drug delivery, and noticeably reduced adverse effects. Gels function as controlled drug delivery systems due to their dispersion component, in which medicine is delivered through a polymer network (a network that is not soluble in water) or supply system (water-insoluble polymeric layer). Organogels, hydrogels, and aerogels serve as supported or regulated drug delivery systems in pharmaceuticals.<sup>93</sup>

#### 2.5.2. Fast release gels:

For quick dissolving pills, gels with superabsorbent and rapid swelling qualities can be used. Acute disorders that call for a quick beginning of action can be treated using fast release gels.<sup>94</sup>

#### 2.5.3. Bioadhesive gels:

The bioadhesive frameworks limit the pharmaceuticals nearby and extend the home season of the medication in the

oral cavity. Bioadhesive gels are used for the delivery of ophthalmic, mucoadhesive, transdermal, vaginal, and cutaneous medications. Cross-connected polyacrylic corrosive gel-framing bioadhesive polymers may adhere to mucosal surfaces for extended periods of time and show regulated drug delivery at the ingesting site. The writing has taken into account several hydrogel-based bioadhesive frameworks for controlled medication release. These types of polymer gel frameworks serve as bioadhesive frameworks and controlled drug delivery devices that may deliver drugs at a specified place with improved bioavailability.<sup>95</sup>

#### 2.5.4. Smart polymer gels:

These also go by the names natural cunning or cunning gels. Specialized professionals are becoming increasingly interested in managed or self-directed delivery platforms for boosts responsive gel. Upgrades sensitive or "shrewd" gels demonstrate an excellent physiochemical shift in reaction to little changes in their present environment, which includes pH, temperature, light, attractive area, and ionic components. These modifications are reversible, so when the indication or reason is removed, the machine may return to its original country. In general, hydrogels react to natural changes, which resemble clever gels.<sup>96</sup>

#### 2.6. Percutaneous absorption and kinetics of drug permeation:

To successfully create topical systems, it is essential to have a solid understanding of skin penetration kinetics. The following procedures are involved in topical medication permeation:

1. Stratum corneum sorption
2. Drug penetration through living skin
3. Drug absorption by the dermal papillary layer's capillary network

If the medicine contains particular physico-chemical characteristics, this penetration may be conceivable. The formula for the rate of permeation over the skin ( $dQ/dt$ ) is

$$dQ / dt = P_s (C_d - C_r) \dots \dots \dots \text{Eq. 1}$$

Where,

$C_d$  = Concentration of skin penetrant in the donar compartment (e.g., on the surface of stratum corneum).

$C_r$  = Concentration in the receptor compartment (e.g., body) respectively.

$P_s$  = Overall permeability constant of the skin tissue to the penetrant.

$$P_s = (K_s D_{ss}) / h_s \dots \dots \dots \text{Eq. 2}$$

Where,

$K_s$  is the partition coefficient for the interfacial partitioning of the penetrant molecule from a solution medium.

$D_{ss}$  is the apparent diffusivity for the steady state diffusion of the penetrant molecule through a thickness of skin tissues  $h_s$  is the overall thickness of skin tissues.

As  $K_s$ ,  $D_{ss}$  and  $h_s$  are constant under given conditions, the permeability coefficient ( $P_s$ ) for a skin penetrant can be considered to be constant.

From Eq.1 it is clear that a constant rate of drug permeation can be obtained only when  $C_d \gg C_r$  i.e., the drug concentration at the surface of the stratum corneum ( $C_d$ ) is consistently and substantially greater than the drug concentration in the body ( $C_r$ ), then Eq. 1 becomes:

$$dQ / dt = P_s C_s \dots \dots \dots \text{Eq. 3}$$

Permeability coefficient =  $(K_s D_{ss}) / h_s = 1 / \text{resistance}$ .<sup>97,98</sup>

#### 2.7. Characteristics of gels:

**Swelling:** Gels have the capacity to swell, absorbing liquid while expanding in size. This might be viewed as the beginning of the disintegration process. Gel-gel interactions are replaced by gel-solvent interactions as a result of solvent permeating the gel matrix. Normal cross-linking in the gel matrix, which inhibits complete disintegration, causes limited swelling. When the solvent combination has a solubility parameter similar to the gallant, this gel expands significantly.<sup>99</sup>

**Syneresis:** After standing, many gel structures experience compression. The interstitial fluid communicates and collects at the gel's top layer. This cycle, known as syneresis, has also been seen in organogels and inorganic hydrogels in addition to natural hydrogels. Syneresis often becomes more pronounced as the polymer cluster gets smaller.

The release of several concerns generated during the gel setting process has been linked to the constriction tool. The interstitial space available for dissolvable decreases as these loads feel much better, forcing the statement of liquid. Osmotic effects have been seen in the syneresis of gels formed from the ionic gel formers gelatin or psyllium seed gum, as well as the effects of pH and electrolyte fixing.<sup>100</sup>

**Ageing:** Colloidal structures often exhibit sluggish unrestrained collection. It is suggested that this connection is developing. When gels mature, a dense organisation of the gelling specialist gradually develops. Since the liquid

medium is removed from the just formed gel, the imer hypothesises that this interaction resembles the initial gelling cycle and continues after the underlying gelation.<sup>101</sup>

**Structure:** The presence of an organisation framed by the interlinking of particles that is a specialist in gelling causes a gel to become hard. The structure of the organisation and the characteristics of gel are determined by the notion of the particles and the type of power responsible for the links. The isolated hydrophilic colloid particles might be made up of discrete macromolecules, spherical or isometric aggregates of small atoms.<sup>102</sup>

**Rheology:** Gelling specialty arrangements and flocculated strong dispersion are examples of fake versatility. Showing Non-Newtonian float conduct is characterised by a decrease in thickness and an increase in shear charge. As n gels mature, a denser organisation of the gelling specialist gradually develops, upsetting the dubious design of inorganic waste dispersed in water.<sup>103</sup>

## 2.8. Evaluation of hydro-gels:

The following criteria were used to assess gels:

- Homogeneity
- Grittiness
- Extrudability study
- pH Determination
- Viscosity
- Skin irritation study
- Drug content
- Spreadability
- *In-vitro* release

### **Homogeneity:**

After the generated gels were placed in the container, they were all visually inspected for homogeneity. They had examinations to check for aggregates and to see how they looked.<sup>104</sup>

### **Grittiness:**

On the off chance that no apparent particulate matter was seen with a light magnifying lens, the four definitions were evaluated infinitesimally for the existence of particles. The gel arrangement so obviously meets the need of independence from particular matter and from coarseness as desired for any efficient preparation.<sup>104</sup>

### **Extrudability:**

A good gel expulsion should preferably have a mild strain applied to the gel. Using a common cylinder filling process, the extrudability of details from aluminium folding cylinders was solved. Two clamps secured an aluminium folding cylinder filled with 10g gels. Extrudability was not completely predetermined in terms of weight in grammes required to release a 0.5 cm lace of gel in 10 seconds from a packed cylinder.<sup>104</sup>

### **pH assurance:**

The use of a computerised pH metre allows the pH of gel to be adjusted. 100 cc of refined was dissolved in 1 gramme of gel before being refrigerated for 2 hours. Every definition's pH was estimated three times, and average characteristics were computed.<sup>105</sup>

### **Viscosity:**

Using a Brookfield Viscometer, the consistency of the pre-assembled gel was estimated. The gel was rotated using shaft number 64 at speeds of 20 and 30, and the corresponding dial reading was recorded.<sup>105</sup>

### **Skin irritancy study:**

For the purpose of testing for skin disturbance, guinea pigs (weighing between 400 and 500g) of both sexes were used. The creatures were fed regular creature food and allowed unrestricted access to the water. The animals were kept in the usual manner. Guinea pigs had their backs' hair removed, and an area of 4 cm<sup>2</sup> was set aside on each side, with one side serving as the control and the other as the test. Two times daily for seven days, gel (500 mg/guinea pig) was applied, and the site's responsiveness and reaction, if any, were noted.<sup>106</sup>

### **Drug content assurance:**

The drug was concentrated by accurately measuring a gel (about 100 mg) and breaking it down in 100 ml of phosphate support 7.4, following which the mixture was continuously blended for 24 hours on an appealing stirrer. Then, the arrangement as a whole was sonified. The medication in the arrangement was evaluated spectrophotometrically by fitting dilution after sonication and subsequent filtering.<sup>106</sup>

### **Spreadability:**

It displays the extent of the area to which the gel quickly spreads upon application to the skin or affected area. The usefulness of a detail also depends on how well-known it is. Spreadability is expressed in terms of the number of seconds it takes two slides to separate from gel that is sandwiched between them while being subjected to a particular

load. Better spreadability is achieved by dividing two slides in less time.<sup>106</sup>

It is calculated by using the formula:

$$S = M \cdot L / T$$

where, M = wt. tied to upper slide

L = length of glass slides

T = time taken to separate the slides.

### ***In -vitro* permeation studies:**

To focus on the disintegration arrival of gels via a cellophane layer, the diffusion studies of the pre-arranged gels were done in a Keshary-Chien dispersion cell. The dispersion review was carried out at 37° using 25 ml of phosphate cradle (pH 7.4) as the disintegration medium, and the gel test (0.5g) was taken in cellophane film. At regular intervals of 1, 2, 3, 4, 5, 6, 7 and 8 hours, 5 ml of each example was taken out and replaced with an equivalent volume of fresh disintegration media. The example was then tested using a phosphate support as a clear at 362 nm for through satisfaction.<sup>107</sup>

### **2.9. Application of gels:**

Gels are used in the pharmaceutical and cosmetic industries.

1. To offer local action, gels are applied directly to the skin, mucous membrane, or eye.
2. They function as implants or intramuscular injections of long-acting medications.
3. Gelling retailers are effective as suppository bases, colloids protectors in suspensions, thickeners in oral liquids, and binders in pill granulation.<sup>108</sup>
4. Cosmetic gels are used in a wide range of products, including shampoos, deodorants, dentifrices, and skin and hair care products.
5. Because the scalp is a region of the body where lotions and ointments are too oily for patients to tolerate, medications containing anti-inflammatory steroids in gel form are used to treat scalp inflammations.
6. Compared to ointments, gels have a better potential as a drug delivery system for topically applied medications since they are robust, nonstick, need less electricity during component operation, and have aesthetic appeal.<sup>103</sup>

### **Conclusion:**

The current review involves a writing survey of effective drug gel structure. Drug gels are two-ease frameworks in which huge natural particles are broken down in the ceaseless stage, arbitrarily looping in the adaptable chains, though inorganic particles are not disintegrated yet only dispersed all through the nonstop stage. Drug gels are many times made by thickening a fluid stage with extra fixings. They are ordinarily made utilizing proper gelling specialists, like HPMC, Carbopol, Sodium CMC, and so forth. Drug gel is made with added substances, like cancer prevention agents, stabilizers, and antimicrobial additives. Taking everything into account, simple spreadability is one of the essential characteristics of any skin drug. Drug Gel is supposed to be successful on the off chance that it spreads across a surface rapidly. Different physicochemical qualities of the advanced gel will be surveyed, including pH, consistency, spreadability, extrudability, drug content, in vitro drug dispersion, ex-vivo bio-glue test, and skin bothering test. The writing survey that was directed for this study uncovered that gel might be an extremely encouraging option in contrast to skin or transdermal treatment. As indicated by a review, drug gel has promising mitigating and wound mending impacts.

**3.1. Acknowledgements:** The authors are thankful to (Prof.) Dr. Sailesh Kumar Ghatuary, Director, Shri RLT Institute of Pharmaceutical Science and Technology, Ekdil-Etawah, Uttar Pradesh, India, for his assistance and providing the valuable suggestions.

**3.2. Availability of data and materials** The datasets used and/or analyzed during the current review are available from the corresponding author on reasonable request.

**3.3. Funding:** Not applicable.

**3.4. Consent for publication:** Not applicable.

**3.5. Competing interests:** The authors declare that they have no competing interests.

**3.6. Conflict of interest:** We declare that we have no conflict of interest.

## REFERENCES

1. Imran K. Tadwee, Sourabh Gore, Prashant Giradkar, Advances in topical drug delivery system: a

- review, *International Journal of Pharmaceutical Research & Allied Sciences*, 2011; 1(1), 14-23.
2. Singh Vijay Kumar, Singh Praveen Kumar, Sharma Purnendu Kumar, Srivastava Peeyush Kumar, Mishra Ashutosh, formulation and evaluation of topical gel of aceclofenac containing piparine, *Indo American Journal of Pharmaceutical Research*, 2013, 3(7), 5266-5280.
  3. Hemendrasinh J Rathod, and Dhruvi P Mehta, A Review on Pharmaceutical Gel, *Acta Scientifica International Journal of Pharmaceutical Science*, 2015, 1(1), 33-47.
  4. Jain N.K. *Pharmaceuticals product Development*. CBS Publishers & Distributors Pvt. Ltd. 2006. First edition : 228-230.
  5. Murdan S. Organogels in drug delivery. *Expert Opin Drug Deliv*. 2005;2:489-505.
  6. Vintiloui A, Leroux JC, Orgnogels and their use in drug delivery: A review. *J Control*
  7. Harper D. "Online Etymology Dictionary: gel". *Online Etymology Dictionary*
  8. Yasir EN, Khashab AL, Yasir MK, Hamadi SA, Al-Waiz MM, Formulation and evaluation of ciprofloxacin as a topical gel, *Asian Journal of Phrr sci*, 8 (2), 2010, 80-95
  9. Stanely S. Transdermal drug delivery. *Mol Interv* 2004; 4(6):308-12.
  10. Girish C. Transdermal drug delivery systems. A review. (Online). 2006 Jan 12 (cited 2009 Jan 12); Available from:
  11. B. Niyaz Basha, Kalyani Prakasam, Divakar Goli, Formulation and evaluation of Gel containing Fluconazole-Antifungal Agent, *International Journal of Drug Development & Research*,2011:3(4), 109-128.
  12. Florence AT, Attwood D. *Physicochemical Principles of Pharmacy*. Pharmaceutical Press, London, UK, 2011.
  13. Cooper and Gunn. "Disperse systems. In: Carter SJ, editor. *Tutorial Pharmacy*". CBS Publishers and Distributors (2000): 68-72.
  14. Bharadwaj Sudhir, Gupta G.D, Sharma V.K. Topical Gel: A Novel approach for drug delivery. *Journal of Chemical Biological and Physical Sciences* 2012; Vol. 2(2): 856-866.
  15. Loyd VA, Nicholas G. Popovich, Howard C. Ansel. "Ansel's pharmaceutical dosage forms and drug delivery systems. 9th ed. Philadelphia: Lippincott Williams & Williams; (2011).
  16. Syeda Ayesha Ahmed un Nabi, Muhammad Ali Sheraz\*, Sofia Ahmed, Nafeesa Mustaan, Iqbal Ahmad, *Pharmaceutical Gels: A Review*, *RADS-JPPS Vol 4 (1)*, June 2016, 40-4.
  17. Suchithra. A. B, S. Jeganath, E. Jeevitha, *Pharmaceutical Gels and Recent Trends –A Review*, *Research J. Pharm. And Tech*. 2019; 12(12): 6181-6186.
  18. Karande P, Mitragotri S: Enhancement of transdermal drug delivery via synergistic action of chemicals, *Biochemica et Biophysica Actas*, 2009, 1788:2362-2373.
  19. Mousumi Kar, Yashu Chourasiya, Rahul Maheshwari, and Rakesh K. Tekade, *basic fundamentals of drug delivery chp-2*, Elsevier Inc, 2019:29-83.
  20. Klein, M.; Poverenov, E. Natural biopolymer-based hydrogels for use in food and agriculture. *J. Sci. Food Agric*. 2020, 100, 2337–2347.
  21. Patil, A.; Ferritto, M.S. Polymers for personal care and cosmetics: Overview. In *Polymers for Personal Care and Cosmetics*; ACS Publications: Washington, DC, USA, 2013; pp. 3–11.
  22. Lochhead, R.Y. *The Role of Polymers in Cosmetics: Recent Trends*; ACS Publications: Washington, DC, USA, 2007.
  23. Kulkarni Vishakha S, Butte Kishor D and Rathod SS: Natural polymers—A comprehensive review. *Int J Res Pharm Biomed Sci* 2012; 3: 1597-13.
  24. Alonso-Sande M, Teijeiro-Osorio D, Remuñán-López C and Alonso MJ: Glucomannan, a promising polysaccharide for biopharmaceutical purposes. *Eur J Pharm Biopharm* 2009; 72: 453-62.

25. Hamman JH: Composition and applications of Aloe vera leaf gel. *Molecules* 2008; 13: 1599-16.
26. Ahad HA: Development and in-vitro evaluation of Glibenclamide Aloe barbadensis Miller leaves mucilage controlled release matrix tablets. *Int. J. Pharm Tech Res* 2010; 2: 1018-21.
27. Langer K: Optimization of the preparation process for human serum albumin (HSA) nanoparticles. *Int J Pharm* 2003; 257: 169-80.
28. Suhail, M.; Hsieh, Y.-H.; Khan, A.; Minhas, M.U.; Wu, P.-C. Preparation and In Vitro Evaluation of Aspartic/Alginate Based Semi-Interpenetrating Network Hydrogels for Controlled Release of Ibuprofen. *Gels* 2021, 7, 68.
29. Nomenclature and Symbolism for Amino Acids and Peptides". IUPAC-IUB Joint Commission on Biochemical Nomenclature. 1983. Archived from the original on 9 October 2008. Retrieved 4 AUG 2022.
30. Valeriy Demchenko, Nataliya Rybalchenko, Svetlana Zahorodnia, Krystyna Naumenko, Sergii Riabov, Serhii Kobylinskyi, Alina Vashchuk, Yevgen Mamunya, Maksym Iurzhenko, Olena Demchenko, Grazyna Adamus, Marek Kowalczyk. Preparation, Characterization, and Antimicrobial and Antiviral Properties of Silver-Containing Nanocomposites Based on Polylactic Acid–Chitosan. *ACS Applied Bio Materials* 2022, 5 (6) , 2576-2585.
31. Lev R, Long R, Mallonga L, Schnaram R and Reily W: Evaluation of Carrageenan as Base for Topical Gels. *Pharm Res* 1997; 14: 42.
32. Kadajji VG and Betageri GV: Water soluble polymers for pharmaceutical applications. *Polymers (Basel)*. 2011; 3: 1972–09.
33. Khalil HPS: Biodegradable polymer films from seaweed polysaccharides: A review on cellulose as a reinforcement material. *Express Polym Lett* 2017; 11.
34. Dijk-Wolthuis VVNE, Hoogbeem JAM, Steenbergen VMJ, Tsang SKY and Hennink WE: Degradation and release behavior of dextran-based hydrogels. *Macromolecules* 1997; 30: 4639-45.
35. De Jong SJ: Biodegradable hydrogels based on stereocomplex formation between lactic acid oligomers grafted to dextran. *J. Control. release* 2001; 72: 47–56.
36. Jantrawut, P. & Ruksiriwanich, Warintorn. (2014). Carbopol®-guar gum gel as a vehicle for topical gel formulation of pectin beads loaded with rutin. *Asian Journal of Pharmaceutical and Clinical Research*. 7. 231-236.
37. Hathout RM and Metwally AA: Gelatin nanoparticles. in *Pharmaceutical Nanotechnology* Springer 2019; 71–78.
38. Cosgrove DJ: Growth of the plant cell wall. *Nat Rev Mol Cell Biol* 2005; 6: 850-61.
39. Ying H: In-situ formed collagen-hyaluronic acid hydrogel as biomimetic dressing for promoting spontaneous wound healing. *Mater Sci Eng C* 2019; 101: 487-98.
40. Kwon MY: Influence of hyaluronic acid modification on CD44 binding towards the design of hydrogel biomaterials. *Biomaterials* 2019; 222: 119451
41. Lin P: Preparation and properties of carboxymethyl chitosan/oxidized hydroxyethyl cellulose hydrogel. *Int J Biol Macromol* 2020; 162: 1692-98
42. Demina TS: Solid-State Synthesis of Water-Soluble Chitosan-g-Hydroxyethyl Cellulose Copolymers. *Polymers (Basel)* 2020; 12: 611
43. Wan X: The physiological functions and pharmaceutical applications of inulin: A review. *Carbohydr Polym* 2020; 116589.
44. Reddy MR: An Introduction to Fast Dissolving Oral Thin Film Drug Delivery Systems: A Review. *J Pharm Sci Res* 2020; 12: 925-40
45. Zhang R: Effects of hydrophobic agents on the physicochemical properties of edible agar/maltodextrin

films. *Food Hydrocoll* 2019; 88: 283-90

46. Ogunsona E, Ojogbo E and Mekonnen T: Advanced material applications of starch and its derivatives. *Eur Polym J* 108: 570–581 (2018).
47. Afshar M, Dini G, Vaezifar S, Mehdikhani M and Movahedi B: Preparation and characterization of sodium alginate/polyvinyl alcohol hydrogel containing drugloaded chitosan nanoparticles as a drug delivery system. *J. Drug Deliv Sci Technol* 2020; 56: 101530.
48. Hasnain MS: Use of alginates for drug delivery in dentistry. in *Alginates in Drug Delivery Elsevier* 2020; 387-04.
49. Kovalenko, S. M. (2017). Prospects of Using Synthetic and Semi-Synthetic Gelling Substances in Development of Medicinal and Cosmetic Gels. *Asian Journal of Pharmaceutics (AJP)*, 11(02).
50. Samala ML, Sridevi G. Role of Polymers as Gelling Agents in the Formulation of Emulgels. *Polym Sci.* 2016, 1:2.
51. Tafuro, G.; Costantini, A.; Baratto, G.; Busata, L.; Semenzato, A. Rheological and Textural Characterization of Acrylic Polymer Water Dispersions for Cosmetic Use. *Ind. Eng. Chem. Res.* 2019, 58, 23549–23558.
52. Erich Penzel (2000). "Polyacrylates". *Ullmann's Encyclopedia of Industrial Chemistry*. Weinheim: Wiley-VCH. doi:10.1002/14356007.a21\_157. ISBN 978-3-527-30673-2.
53. De Silva DJ, Olver JM (July 2005). "Hydroxypropyl methylcellulose (HPMC) lubricant facilitates insertion of porous spherical orbital implants". *Ophthal Plast Reconstr Surg.* **21** (4): 301–2.
54. National Center for Biotechnology Information (2022). PubChem Compound Summary for CID 24846132, Hydroxyethyl cellulose. Retrieved August 4, 2022.
55. Ohara, Takashi; Sato, Takahisa; Shimizu, Noboru; Prescher, Gunter; Schwind, Helmut; Weiberg, Otto; Marten, Klaus; Greim, Helmut (2020). *Acrylic Acid and Derivatives*. doi:10.1002/14356007.a01\_161.pub4. ISBN 978-3527306732. OCLC 910197915. S2CID 213437320. Archived from the original on 19 December 2021.
56. Patil, A.; Sandewicz, R.W. *Cosmetic science and polymer chemistry: Perfect together*. In *Polymers for Personal Care and Cosmetics*; American Chemical Society: Washington, DC, USA, 2013; Volume 1148, pp. 13–37.
57. Iunchedii, P.; Juliano, C.; Gavin, E.; Cossu, M.; Sorrenti, M. In vivo formulation and testing of chlorhexidine buccal tablets prepared using drug-loaded chitosan microspheres. *Eur. UJ. Pharm. Biopharm.* 2002, 53, 233239.
58. Mohite, BV; Patil, S.V. The biomaterial of the novel: Bacterial cellulose and its applications for the new era. *Bioethanol. The Biochem app.* 2014, 61, 101-110.
59. Costa, C.; Medronho, B.; Philip, A.; Mira, mine.; Lindman, B.; Edlund, H.; Norgren, M. Emulsion Formation and Stabilization by Biomolecules: The Leading Role of Cellulose. *Polymers* 2019, 11, 1570.
60. Iijima, M.; Hatakeyama, T.; Hatakeyama, H. Gel-sol – gel is a modification of kappa-carrageenan and methylcellulose binary systems studied with different scanning calorimetry. *Thermochim. Acta* 2014, 596, 6369.
61. Goddard, E.D.; Gruber, J.V. *Principles of Polymer Science and Technology in Cosmetics and P Care*; CRC Press: Boca Raton, FL, USA, 1999.
62. Kumar-Sarangi, M.; Chandra-Joshi, B.; Ritchie, B. Dealers of natural bio enhancers in drug delivery: Overview *P. R. Health Sci. UJ.* 2018, 37,
63. Murugesh Babu, K. 7 – Spider silk and its use. *Silk*; Murugesh Babu, K., Ed.; Woodhead Publishing: Sawston, UK, 2013; pages 156-176.

64. Halasa, A. F. (1981). "Recent Advances in Anionic Polymerization". *Rubber Chemistry and Technology*. 54 (3): 627–640. doi:10.5254/1.3535823.
65. Haiyan Zheng; Baoqi Zuo; (2021). Functional silk fibroin hydrogels: preparation, properties and applications. *Journal of Materials Chemistry B*, (), -. doi:10.1039/d0tb02099k
66. Jiang, S., Liu, S., Feng, W., 2011. PVA hydrogel properties for biomedical application. *Journal of the Mechanical Behavior of Biomedical Materials* 4, 1228-1233.
67. Hosmani, Avinash & Thorat, Y.S & Kasture, P.V. (2006). Carbopol and its Pharmaceutical Significance: A Review. *Pharmaceutical Reviews*. 4.
68. Shastri, V.P., 2003. Non-degradable biocompatible polymers in medicine: past, present and future. *Current Pharmaceutical Biotechnology* 4, 331-337.
69. Ubaid, M., Ilyas, S., Mir, S., Khan, A. K., Rashid, R., Khan, M. Z., Kanwal, Z. G., Nawaz, A., Shah, A., & Murtaza, G. (2016). Formulation and in vitro evaluation of carbopol 934-based modified clotrimazole gel for topical application. *Anais da Academia Brasileira de Ciencias*, 88(4), 2303–2317. <https://doi.org/10.1590/0001-3765201620160162>.
70. Schacht, E., Vandorpe, J., Crommen, J., Seymour, L., 1996. In: Ogata, N., Kim, S.W., Feijen, J., Okano, T. (Eds.), *Biodegradable Polyphosphazenes for Biomedical Applications BT - Advanced Biomaterials in Biomedical Engineering and Drug Delivery Systems*. Springer Japan, Tokyo, pp. 81-85.
71. Safitri, Fenny & Nawangsari, Desy & Febrina, Dina. (2021). Overview: Application of Carbopol 940 in Gel. 10.2991/ahsr.k.210127.018
72. Muramatsu, Mitsuo & Kanada, Ken & Nishida, Ayumu & Ouchi, Kiyohisa & Saito, Noriyasu & Yoshida, Minoru & Shimoaka, Akihiro & Ozeki, Tetsuya & Yuasa, Hiroshi & Kanaya, Yoshio. (2000). Application of Carbopol (R) to controlled release preparations I. Carbopol (R) as a novel coating material. *International journal of pharmaceutics*. 199. 77-83. 10.1016/S0378-5173(00)00374-4.
73. Woerly, S., Pinet, E., De Robertis, L., Bousmina, M., Laroche, G., Roitback, T., Vargova, L., Sykova, E., 1998. Heterogeneous PHPMA hydrogels for tissue repair and axonal regeneration in the injured spinal cord. *Journal of Biomaterials Science, Polymer Edition* 9, 681-711.
74. Burke, A., Hasirci, N., 2004. In: Hasirci, N., Hasirci, V. (Eds.), *Polyurethanes in Biomedical Applications BT - Biomaterials: From Molecules to Engineered Tissue*. Springer US, Boston, MA, pp. 83-101.
75. Aguilar M.R., Elvira C., Gallardo A., Vázquez B., Román J.S. Smart Polymers and Their Applications as Biomaterials. In: Ashammakhi N., Reis R.L., Chiellini E., editors. *Topics in Tissue Engineering. Volume 3 Biomaterials and Tissue Engineering Group*; Oulu, Finland: 2007
76. Teo, A.J.T., Mishra, A., Park, I., Kim, Y.-J., Park, W.-T., Yoon, Y.-J., 2016. Polymeric biomaterials for medical implants and devices. *ACS Biomaterials Science and Engineering* 2, 454-472.
77. Ferreira, P., Silva, A.F.M., Pinto, M.I., Gil, M.H., 2008. Development of a biodegradable bioadhesive containing urethane groups. *Journal of Materials Science: Materials in Medicine* 19, 111-120.
78. Maitz, M.F., 2015. Applications of synthetic polymers in clinical medicine. *Biosurface and Biotribology* 1, 161-176.
79. Klinkmann, H., Vienken, J., 1995. Membranes for dialysis. *Nephrology Dialysis Transplantation* 10, 39e45.
80. G. Aggarwal. M. Nagpal, *Pharmaceutical Polymer Gels in Drug Delivery-chp-10*, Springer Nature Singapore Pte Ltd., 2018:249-284.
81. Prem Samundre, Surendra Dangi, Teena Patidar, Shubham Maroti Shende, a review on topical gel, *International Journal of Creative Research Thoughts*, 2020:8(4), 3951-3954.

82. Labarre D, Ponchel G, Vauthier C. Biomedical and Pharmaceutical Polymers. Pharmaceutical Press, London, UK, 2010.
83. Gad SC. Pharmaceutical Manufacturing Handbook: Production and Processes. Wiley-Blackwell, Hoboken, USA, 2008.
84. Bhowmik Debjit, Gopinath Harish, Kumar B. Pragati, Duraivel S, Kumar KP Sampath. Recent Advances in Topical Drug Delivery System. The Pharma. Innovation Journal 2012; Vol. 1(9): 12.
85. Vollmert B. Polymer Chemistry. Springer Science & Business Media, New York, USA, 2011.
86. Syeda Ayesha Ahmed un Nabi, Muhammad Ali Sheraz, Sofia Ahmed, Nafeesa Mustaan, Iqbal Ahmad, Pharmaceutical Gels: A Review, RADS-JPPS Vol 4 (1), 2016, 40-48.
87. K.A. Davis, K.S.Anseth, Controlled release from cross linked degradable networks, Criti. Rev. Ther. Drug Carr, Syst. 2002; 19; 385-423.
88. Kumar Ajay. Badde Shital., Kamble Ravindra, Development and Characterization of liposomal drug delivery system for nimesulide; IJPPS.2010; 2(4); 87-89.
89. Prabhjotkaur, Loveleenpreetkaur and MU. Khan, Topical formulations and Hydro-gel: An overview, international journal of advances in pharmacy,biology and chemistry,2013; 2(1),201-206.
90. Shaik Arif basha et.al, recent trends in usage of polymers in the formulation of dermatological gels, Indian Journal of Research in Pharmacy and Biotechnology, 2013:1(2), 161-168.
91. <http://en.wikipedia.org>. Gel Available from: <http://en.wikipedia.org/wiki/Gel>
92. Loveleen Preet Kaur, Tarun Kumar Guleri, Topical Gel: A Recent Approach for Novel Drug delivery, Asian Journal of Biomedical and Pharmaceutical Sciences, 2013: 3(17),1-5.
93. Li, J., & Mooney, D. J. (2016). Designing hydrogels for controlled drug delivery. Nature reviews. Materials, 1(12), 16071. <https://doi.org/10.1038/natrevmats.2016.71>
94. Venkatesh, M. P., Kumar, T. P., & Pai, D. R. (2020). Targeted drug delivery of Methotrexate in situ gels for the treatment of Rheumatoid Arthritis. Saudi pharmaceutical journal : SPJ : the official publication of the Saudi Pharmaceutical Society, 28(12), 1548–1557. <https://doi.org/10.1016/j.jsps.2020.10.003>
95. Reddy PC, Chaitanya KSC, Rao YM (2011) A review on bioadhesive buccal drug delivery systems: current status of formulation and evaluation methods. Daru 19(6):385–403.
96. Almeida H, Amaral MH, Lobão P (2012a) Temperature and pH stimuli-responsive polymers and their applications in controlled and selfregulated drug delivery. J Appl Pharm Sci 2(06):1–10.
97. Shah VP, Maibach HI, Topical Drug Bioavailability, Bioequivalence, and Penetration, 1, Springer, USA, 1993, 369-391.
98. Robinson JR, VHL Lee, Controlled drug delivery: Fundamentals and applications, 2, Marcel Dekker Inc., New York, 1987, 523-552.
99. Cooper and Gunn. “Disperse systems. In: Carter SJ, editor. Tutorial Pharmacy. CBS Publishers and Distributors (2000): 68-72.
100. Haghghi, M., & Rezaei, K. (2012). General analytical schemes for the characterization of pectin-based edible gelled systems. TheScientificWorldJournal, 2012, 967407.
101. Zatz JL., et al. “Pharmaceutical dosage form: Disperse system”. Marcel Dekker (2005): 399-421.
102. Ashni Verma, Sukhdev Singh, Rupinder Kaur, Upendra K Jain, Topical Gels as Drug Delivery Systems: A Review, International Journal of Pharmaceutical Sciences Review and Research, 2013; 23(2), 374-382.
103. Lieberman HA, Rieger MM, Banker GS, Pharmaceutical dosage form: Disperse system, 2, Marcel Dekker, New York, 2005, 399-421.
104. Banker.G.S. and Rhodes. C.T., Moderen Pharmaceutics, 2<sup>nd</sup> Edn.,vol.40,Marcel Dekker,inc,

Madison avenue .New York, 1990,303-307.

105. Martinez MAR, Gallardo JLV, Benavides MMD, Duran JDGL, Lara V G; Rheological behavior of gels and meloxicam release . Int J Pharm; 2007; 333; 17-23.
106. Garg A, Aggarwal D, Garg S, Singla A K; Spreading of semisolid Formulations; An update. Pharm Tech 2002; 84-104
107. Inflammation (Wikipedia, the free encyclopedia).
108. Yamaguchi Y, Sugibayashi K, Morimoto Y; drug release test to asses quality of topical formulations in Japanese market. Drug Dev Ind Pharm 1996; 22(7): 569-577.
109. Shah VP, Maibach HI, Topical Drug Bioavailability, Bioequivalence, and Penetration, 1, Springer, USA, 1993, 369-391.